

Fig. 12 Velocity of Micro-wheel under Sliding Mode Control

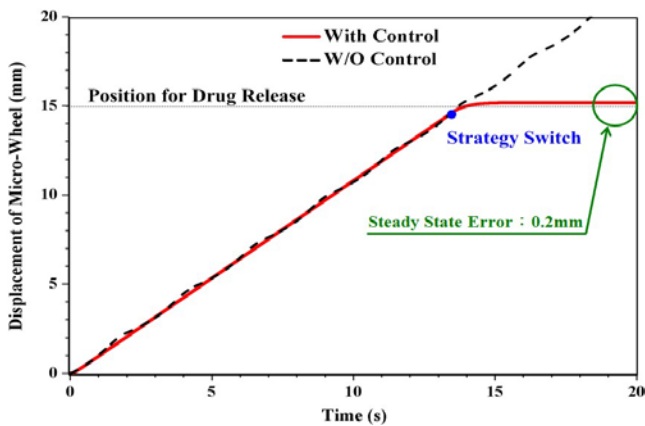


Fig. 13 Displacement of Micro-wheel under Sliding Mode Control

At the beginning, *Control Strategy I* is engaged since the micro-wheel is far away from the drug-release spot. From Fig. 12, it can be observed that the velocity of micro-wheel is increased to the desired velocity and then retained at a constant speed. In addition, the jerk, which occurs under open-loop circumstance, has been successfully suppressed. On the other hand, as the micro-wheel comes close to the drug-release spot, *Control Strategy II* is engaged to replace *Control Strategy I* so that the micro-wheel is slowed down and finally stops at the drug-release spot. To sum up, the expected performance of the micro-wheel is quite satisfactory. The corresponding control current to realize the motion of micro-wheel in Fig. 13 is shown in Fig. 14.

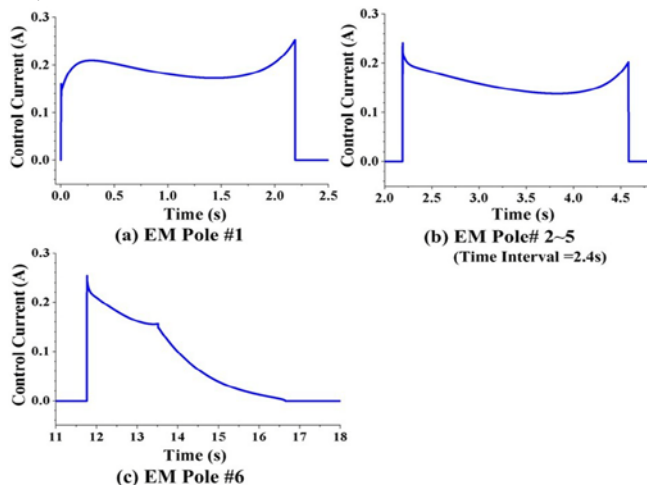


Fig. 14 Control Current of EM Poles in Sequence

The applied control currents at *EM Poles #2-5* are identical, and the time interval between any two adjacent poles energized in shift is 2.4 seconds. Moreover, the maximum of the control current is limited by 0.25 A to avoid burn-up of the coils at EM poles.

V. CONCLUSION

A drug-delivery micro-wheel system, composed by an auto-rolling micro-wheel and a micro-drug release mechanism, is proposed. First of all, the micro-wheel is designed to possess the simple characteristics of movement and small size (maximum diameter under 5 mm). By taking advantage of strong driving force provided by magnetic poles in which the iron cores are embedded inside, the micro-wheel is able to roll over rapidly. The average velocity can reach 1.094 mm/sec under applied current 0.2 A at EM (Electro-magnetic) poles. Secondly, the commercial software, *Ansoft Maxwell*, is employed to verify the proposed design of EM poles such that the numbers of the micro-solenoids and windings of the coils are the best for realization of the micro-wheel by taking cost and overall size into consideration. Finally, two strategies based on sliding mode control for the micro-wheel rotation are developed and verified by intensive computer simulations. Not only the micro-wheel can move to the drug-release spot precisely, but also the jerk, which occurs under open-loop circumstance, can be successfully suppressed. To sum up, the proposed MEMS-based micro-wheel theoretically has the potential to fulfill micro-drug-delivery applications in medical service.

ACKNOWLEDGMENT

The authors thank for the financial support and the equipments access which National Science Council (NSC) and National Nano Device Laboratories (NDL) have provided. (Projects: NSC 100-2221-E-006-236- and NDL 100-C02M3-020)

REFERENCES

- [1] B. R. Donald, G. Levey, G. McGray, I. Paprotny and D. Rus, "An Untethered Electrostatic Globally Controllable MEMS Micro-Robot," *Journal of Microelectromechanical Systems*, Vol. 15, No. 1, pp. 1-15, 2006.
- [2] M. H. Mohebbi, M. L. Terry and K. F. Böhringer, "Omnidirectional walking microrobot realized by thermal microactuator arrays," *ASME International Mechanical Engineering Congress and Exposition*, Vol. 2, pp. 2741-2747, 2001.
- [3] H. David and G. Michael, "Robotic micro-assembly of microparts using a piezogrripper," *IEEE/RSJ International Conference on Intelligent Robots and Systems*, pp. 4042-4047, 2008.
- [4] C. H. Ahn, M. G. Allen, "Micromachined planar inductors on silicon wafers for MEMS applications," *IEEE Transactions on Industrial Electronics*, Vol. 45, No. 6, pp. 866-876, 1998.
- [5] K. Noguchi, H. Fujita, M. Suzuki and N. Yoshimura, "The measurements of friction on micromechatronics elements," *IEEE Micro Electro Mechanical Systems*, pp. 148-153, 1991.